

# Design and Synthesis of a Calcium-Sensitive Photocage

Laurel M. Heckman, Jonathan B. Grimm, Eric R. Schreiter, Charles Kim, Mark A. Verdecia, Brenda C. Shields, and Luke D. Lavis\*

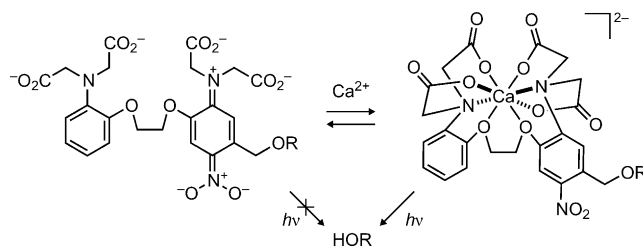
**Abstract:** Photolabile protecting groups (or “photocages”) enable precise spatiotemporal control of chemical functionality and facilitate advanced biological experiments. Extant photocages exhibit a simple input–output relationship, however, where application of light elicits a photochemical reaction irrespective of the environment. Herein, we refine and extend the concept of photolabile groups, synthesizing the first  $\text{Ca}^{2+}$ -sensitive photocage. This system functions as a chemical coincidence detector, releasing small molecules only in the presence of both light and elevated  $[\text{Ca}^{2+}]$ . Caging a fluorophore with this ion-sensitive moiety yields an “ion integrator” that permanently marks cells undergoing high  $\text{Ca}^{2+}$  flux during an illumination-defined time period. Our general design concept demonstrates a new class of light-sensitive material for cellular imaging, sensing, and targeted molecular delivery.

Small molecules that absorb light have broad utility as tools to probe and perturb biological systems. Chemical fluorophores constitute one important type of light-absorbing molecule.<sup>[1]</sup> The ability to modify dyes using chemistry allows the construction of numerous probes for specific applications. For example, changing the chemical structure of fluorophores can allow fine-tuning of spectral properties. Likewise, chemical dyes that respond to changes in ion concentration have been prepared. The design and synthesis of such ion indicators involves incorporation of molecular recognition motifs into a fluorophore where the reversible binding of a specific ion alters the absorption and/or fluorescence quantum yield of the dye. This strategy has produced probes for many biologically relevant ions, including  $\text{Na}^+$ ,  $\text{K}^+$ ,  $\text{Mg}^{2+}$ ,  $\text{Ca}^{2+}$ , and  $\text{Zn}^{2+}$ , allowing noninvasive monitoring of ion concentration inside living cells.<sup>[2]</sup>

Photolabile protecting groups or “photocages” comprise another important class of organic chromophore where photon absorption elicits cleavage of a chemical bond.<sup>[3]</sup> Like fluorophores, the spectral properties of photocages have been manipulated using chemistry, resulting in photolabile groups with longer wavelengths and larger two-photon

cross-sections.<sup>[4]</sup> However, unlike fluorescent dyes, the incorporation of ion-sensitive motifs into photocages is essentially unexplored. Probes built from ion-sensitive photolabile groups could complement reversible ion indicators, functioning as chemical coincidence detectors that would selectively and irreversibly release a small molecule only in the presence of both light and increased ion concentration. In particular, caging a fluorophore with such an ion-sensitive photocage would yield a fluorescent ion “snapshot indicator” or “integrator” that would permanently record increased ion concentration during an illumination-defined time period. Integrator systems based on fluorescent proteins<sup>[5]</sup> and rhodopsins<sup>[6]</sup> have been described recently, but small-molecule ion integrators remain unknown. This currently limits the use of such probes to biological systems that are amenable to genetic manipulation. Herein we describe the design and synthesis of the first  $\text{Ca}^{2+}$ -sensitive photocage. Caging a coumarin fluorophore with this moiety yields a probe that exhibits a 600-fold increase in photochemical quantum yield upon binding  $\text{Ca}^{2+}$ . This compound can serve as an ion integrator that permanently marks neurons undergoing increased  $[\text{Ca}^{2+}]$  elicited by ionophore treatment or electrical stimulation.

Nearly all small-molecule  $\text{Ca}^{2+}$  indicators utilize the calcium-ion chelator moiety 1,2-bis(*o*-aminophenoxy)ethane-*N,N,N',N'*-tetraacetic acid (BAPTA) developed by Tsien.<sup>[7]</sup> To fashion a  $\text{Ca}^{2+}$ -sensitive photocage we envisioned incorporating an *o*-nitrobenzyl photolabile group into BAPTA as shown in Scheme 1. In the absence of  $\text{Ca}^{2+}$ , we



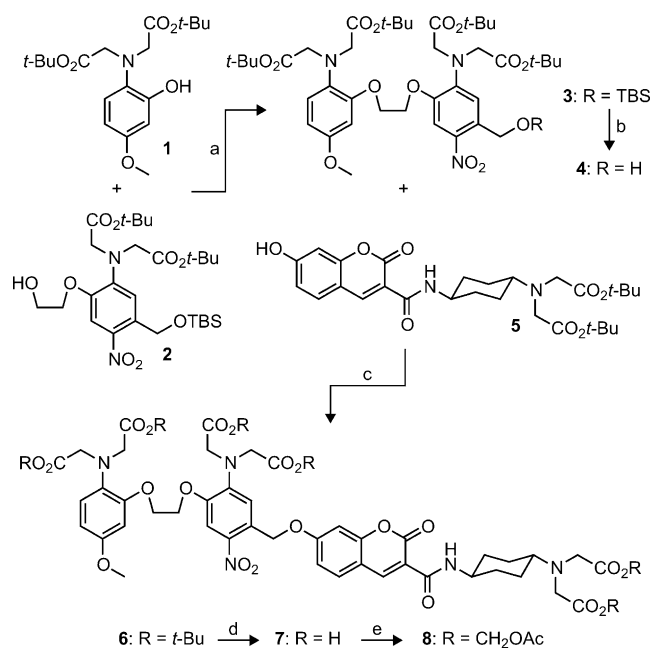
**Scheme 1.** Design of a  $\text{Ca}^{2+}$ -dependent photocage.

surmised that the *para*-nitroaniline ring would adopt a charge-separated colored quinoid form, which exhibits a low-lying triplet state,<sup>[8]</sup> thus suppressing photochemical release. Both nitrobenzyl and nitroindoline cages containing *p*-dialkylamino substituents display low photochemical quantum yields ( $\Phi$ ).<sup>[9]</sup> We expected  $\text{Ca}^{2+}$  binding would reverse this effect as the aniline nitrogen lone pair participates in chelation. This would recapitulate the *o*-nitrobenzyl electronic structure and increase the  $\Phi$  value.

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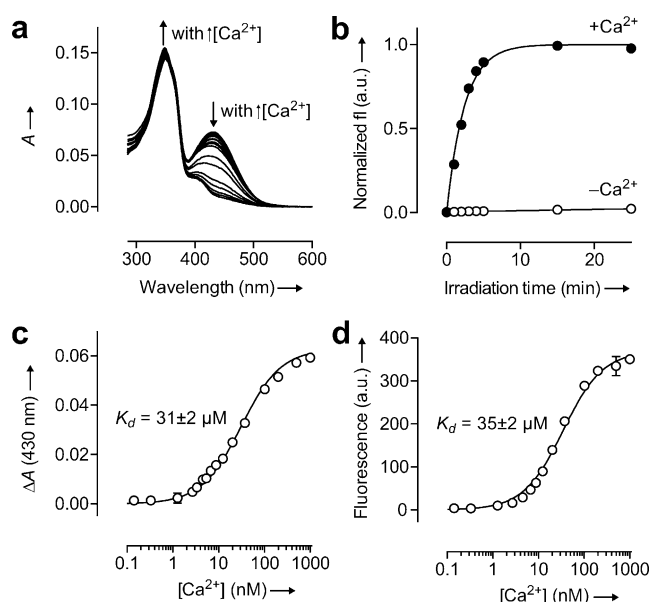
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**Scheme 2.** Synthesis of Ca<sup>2+</sup>-dependent photocaged coumarin **7** and permeable derivative **8**. a) DIAD, PPh<sub>3</sub>, THF, 80%. b) TBAF, THF, 95%. c) DIAD, PPh<sub>3</sub>, THF, 71%. d) TFA, CH<sub>2</sub>Cl<sub>2</sub>, 84%. e) BrCH<sub>2</sub>OAc, DIEA, DMF, 51%. DIAD = diisopropyl azodicarboxylate; TBAF = tetrabutylammonium fluoride; TFA = trifluoroacetic acid; DIEA = *N,N*-diisopropylethylamine; TBS = *tert*-butyldimethylsilyl.

As a result of the intricacy of this molecular system, we developed a facile, modular synthesis of the Ca<sup>2+</sup>-sensitive photocage and first-generation integrator as shown in Scheme 2. We prepared phenol **1** and alcohol **2** through efficient 4- and 7-step syntheses, respectively (see Scheme S1 in the Supporting Information). The key step in our convergent route is a high-yielding Mitsunobu reaction between these atypical coupling partners to give bis-phenoxyethane **3**. The electron-donating methoxy substituent on module **1** was incorporated to balance the requisite electron-withdrawing nitro group on component **2** and maintain a biologically relevant equilibrium dissociation constant ( $K_d$ ) for Ca<sup>2+</sup>.<sup>[7b]</sup> Compound **3** was selectively deprotected to give benzyl alcohol **4**. Attachment of coumarin **5**<sup>[10]</sup> yielded **6**, which could be deprotected to afford Ca<sup>2+</sup>-dependent photocaged coumarin **7**.

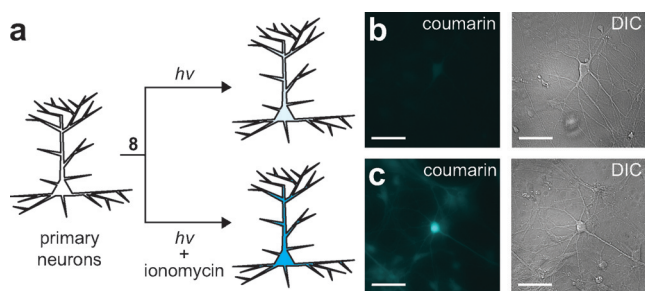
We first examined the absorption spectrum of **7** in buffers containing varying Ca<sup>2+</sup> ion concentrations (Figure 1a). The absorption in the visible region at  $\lambda = 430$  nm shows a dramatic decrease as [Ca<sup>2+</sup>] increases. We also observe a small (less than 5%) but significant increase in absorption around 350 nm when the calcium ion concentration is raised. However, the coumarin moiety dominates absorption in the UV region with an extinction coefficient  $\epsilon = 2.4 \times 10^4 \text{ M}^{-1} \text{ cm}^{-1}$  at  $\lambda = 350$  nm. These absorbance changes support our hypothesis that chelation of calcium would cause a switch from the colored quinoid form to the UV-absorbing aromatic form (Scheme 1). We then investigated the Ca<sup>2+</sup> dependence of the photochemical reaction of compound **7** in vitro where we observed efficient photochemistry only in the presence of



**Figure 1.** Properties of the calcium-sensitive photocage. a) Absorbance spectra of **7** in aqueous buffers containing different [Ca<sup>2+</sup>]. b) Normalized fluorescence intensity (fl) of released coumarin versus irradiation time (irradiating at  $\lambda = 365$  nm) of **7** in the presence (●; 10 mM CaCl<sub>2</sub>) or absence (○; 10 mM ethylene glycol tetraacetic acid (EGTA)) of Ca<sup>2+</sup> ions. c) Determination of the  $K_d$  value of compound **7** by the change in absorbance at  $\lambda = 430$  nm ( $\Delta A$ ). d) Determination of the  $K_d$  value of compound **7** by the initial fluorescence increase. Error bars in (b–d) show  $\pm$  the standard error (S.E.;  $n = 2$ ).

calcium ions (Figure 1b). Under illumination with light of wavelength  $\lambda = 365$  nm, the photocaged fluorophore **7** exhibited  $\Phi$  values of 0.008 % and 4.8 % in the absence or presence of Ca<sup>2+</sup>, respectively. This 600-fold enhancement in quantum yield further validates our molecular design. We determined the calcium ion affinity of compound **7** by measuring, as a function of [Ca<sup>2+</sup>], the change in absorbance at  $\lambda = 430$  nm (Figure 1c) or the initial fluorescence increase from photoactivation (Figure 1d). We found  $K_d$  values of 31 and 35  $\mu\text{M}$  for the absorbance and fluorescence measurements, respectively, consistent with the nitro and methoxy substituents on the BAPTA system.<sup>[7b]</sup> To ensure generality of this approach we prepared an analogous compound based on the dye Tokyo Green (Scheme S2) and observed  $\Phi_{-Ca} = 0.011$  % and  $\Phi_{+Ca} = 1.6$  % (150-fold enhancement) with similar affinity ( $K_d = 28 \mu\text{M}$ ; Figure S1). Photocaged coumarins are known to exhibit higher photochemical quantum yields than other photoactivatable fluorophores as a result of efficient energy transfer from the coumarin chromophore to the photolabile cage moiety.<sup>[10,11]</sup>

We next examined the utility of this system in a cellular context. The hexa-acetoxymethyl (AM) ester of compound **7** was prepared (**8**; Scheme 2). This cell-permeant compound enabled loading of cultured hippocampal neurons with the calcium-sensitive photocaged dye. Cells were washed and then treated with normal media or media containing ionomycin, followed by illumination with activating light (Figure 2a). The overlap of the photo-uncaging wavelength ( $\lambda_{\text{max}} = 351$  nm) with the absorption band of the released



**Figure 2.** Function of  $\text{Ca}^{2+}$ -sensitive photocaged coumarin in neurons. a) Representation showing the experimental setup. b, c) Fluorescence (left) and differential interference contrast (DIC) microscopy images (right) of live cultured hippocampal neurons incubated with AM ester **8** ( $10\ \mu\text{M}$ ) for 1 h and then illuminated with light of wavelength  $\lambda = 365\ \text{nm}$  for 20 s. Scale bars =  $100\ \mu\text{m}$ . b) Untreated neurons. c) Neurons treated with ionomycin.

coumarin ( $\lambda_{\text{max}} = 402\ \text{nm}$ ) allowed simultaneous imaging and activation with a single light source centered at  $\lambda = 365\ \text{nm}$ . Illumination of control cells elicited a relatively small fluorescence increase (Figure 2b). In contrast, cells pretreated with ionomycin showed a 40-fold increase in the accumulation of cellular fluorescence (Figure 2c; Figure S2). Similar results were observed in human embryonic kidney (HEK) cells (Figure S3).

We then investigated if this approach could measure calcium ion changes in neurons induced by electrical stimulation. Low-affinity reversible  $\text{Ca}^{2+}$  indicators are advantageous for studying biological systems as their low buffering capacity preserves native calcium ion dynamics.<sup>[12]</sup> Nevertheless, the inherently poor signal-to-background ratios of such indicators typically restrict their utility to subcellular compartments undergoing extremely high calcium flux (for example, dendritic spines).<sup>[13]</sup> We hypothesized that the permanent signal afforded by the ion integrator would allow measurement of smaller changes in cellular calcium levels using this non-perturbative, low-affinity probe.

To further support this prediction, we modeled the expected release rate of compound **7** under different  $\text{Ca}^{2+}$  concentrations using Equation (1):

$$k = I(\sigma_f C_f \Phi_f + \sigma_b C_b \Phi_b) \quad (1)$$

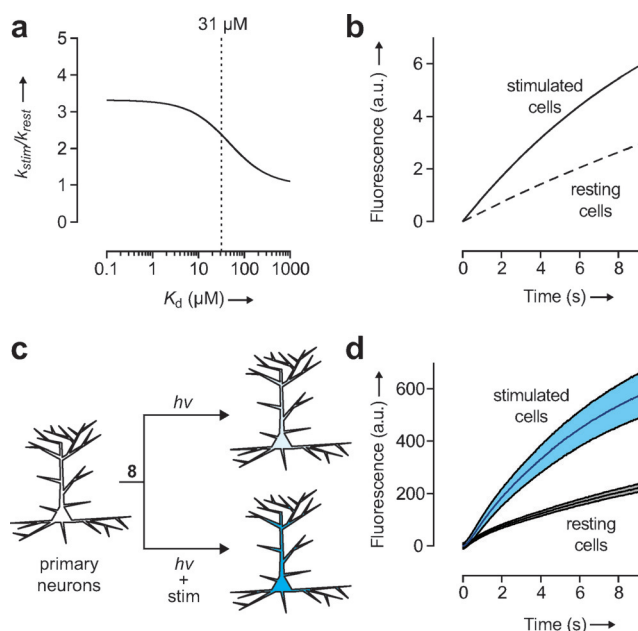
where  $k$  = the rate of photochemical reaction,  $I$  = the intensity of light,  $\sigma$  = the decadic extinction coefficient,  $C$  = the concentration of indicator,  $\Phi$  = the photochemical quantum yield, and subscripts  $b$  and  $f$  indicate  $\text{Ca}^{2+}$ -bound and  $\text{Ca}^{2+}$ -free, respectively. From mass action (see the Supporting Information), the concentration of bound indicator ( $C_b$ ) can be calculated using Equation (2):

$$C_b = \frac{(C_t + [\text{Ca}^{2+}]_t + K_d) - \sqrt{(C_t + [\text{Ca}^{2+}]_t + K_d)^2 - 4(C_t[\text{Ca}^{2+}]_t)}}{2} \quad (2)$$

where  $C_t$  = total concentration of indicator,  $[\text{Ca}^{2+}]_t$  is the total calcium ion concentration in the cells, and  $K_d$  is the dissociation constant of the  $\text{Ca}^{2+}$ -sensitive photocage indicator. The concentration of free indicator ( $C_f$ ) can be calculated

from  $C_t$  and  $C_b$  values. We first modeled the rate of uncaging in stimulated cells relative to the rate in resting cells ( $k_{\text{stim}}/k_{\text{rest}}$ , the uncaging contrast) as a function of  $K_d$  value, assuming average  $\text{Ca}^{2+}$  ion concentrations of  $245\ \text{nM}$  and  $62\ \text{nM}$  in stimulated and resting cells, respectively,<sup>[14]</sup> and an indicator concentration ( $C_t$ ) of  $10\ \mu\text{M}$  (Figure 3a). Under these conditions, the maximum achievable contrast is predicted to be 330%. This value is largely dictated by the approximately fourfold increase in  $\text{Ca}^{2+}$  concentration and noncooperative binding of BAPTA (Hill coefficient = 1). Moreover, our mathematical modeling predicts that decreasing the  $K_d$  value has only a modest effect on contrast; compound **7** ( $K_d = 31\ \mu\text{M}$ ) should still give a  $k_{\text{stim}}/k_{\text{rest}}$  value of 240% (Figure 3a) resulting in a clear delineation of stimulated and unstimulated cells (Figure 3b). This magnitude of photochemical contrast is similar to the change in fluorescence over resting fluorescence ( $\Delta F/F_0$ ) achieved with reversible small-molecule  $\text{Ca}^{2+}$  indicators in cells (typically less than 300%). However, we note the integrating-type measurement of the  $\text{Ca}^{2+}$ -sensitive photocage yields a permanent rather than transient fluorescent signal.

We then tested this prediction in living cells with the experimental design shown in Figure 3c. Cells were incubated with AM ester **8** and subjected to the photoactivation-imaging procedure as before. In one population of cells we elicited neuronal action potential firing by field stimulation at 80 Hz.



**Figure 3.** Theoretical and experimental performance of the  $\text{Ca}^{2+}$ -sensitive photocage as an ion integrator. a) Plot showing the theoretical uncaging contrast ( $k_{\text{stim}}/k_{\text{rest}}$ ) as a function of  $K_d$ . Dashed line shows the  $K_d$  value for compound **7** ( $31\ \mu\text{M}$ ). b) Theoretical rate of fluorescence intensity increase using probe **7** in cells, assuming an average  $[\text{Ca}^{2+}]$  of  $245\ \text{nM}$  and  $62\ \text{nM}$  in stimulated and resting cells, respectively. c) Schematic representation showing the experimental setup. d) Plot of the increase in cellular fluorescence intensity versus irradiation time of cultured neurons without electrical stimulation (gray;  $k = 0.0325\ \text{s}^{-1}$ ) and with stimulation (cyan;  $k = 0.133\ \text{s}^{-1}$ ). Shading shows  $\pm$  S.E. ( $n = 20$ ).

This electrical stimulation caused a significant rate increase in signal relative to unstimulated cells, giving a permanent, 200% larger  $\Delta F$  in stimulated cells (Figure 3d). These experimental rates are similar to those predicted (Figure 3b), validating the mathematical model.

In summary, we have designed and synthesized the first  $\text{Ca}^{2+}$ -sensitive photocage and demonstrated a new paradigm for sensing using small-molecule ion integrators. Our probe exhibits high photochemical contrast, functions in a cellular context, and can sense biologically relevant calcium ion levels. This new class of small-molecule  $\text{Ca}^{2+}$  indicator yields a permanent fluorescent signal that could enable simpler assays for high-throughput screening or the post hoc mapping of active cells in genetically intractable organisms. Additionally, our modular synthetic strategy should facilitate improvements to this probe, such as modulating the  $\text{Ca}^{2+}$  affinity,<sup>[2d,15]</sup> altering the properties of the released fluorophore,<sup>[16]</sup> increasing the two-photon cross-section of the photocage by using the indoline scaffold,<sup>[9a,17]</sup> and changing selectivity to other ions that are similarly unable to elicit chemical reactions on their own (e.g.,  $\text{Na}^+$ ).<sup>[2c,18]</sup> Finally, unlike the genetically encoded systems,<sup>[5,6]</sup> the flexibility of this small-molecule scaffold opens the door for pharmacological agents or chemical gene inducers to be photocaged and released using a “functional photochemistry” approach, allowing sophisticated biological experiments where active cells are selectively targeted for chemical manipulation.

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